The Effects of Stabilization and McKenzie Exercises on Transverse Abdominis and Multifidus Muscle Thickness, Pain, and Disability: A Randomized Controlled Trial in NonSpecific Chronic Low Back Pain

MOHAMMAD HOSSEINIFAR, PhD Candidate1), MOHAMMAD AKBARI, PhD1)*, HAMID BEHTASHI, MD2), MOHSEN AMIRI, PhD3), JAVAD SARRAFZADEH, PhD1)

1) Department of Physical Therapy, Tehran University of Medical Sciences: P.O. Box: 1545913187, Tehran, Iran
2) Department of Orthopedy, Tehran University of Medical Sciences, Iran
3) Department of Physical Therapy, University of Welfare and Rehabilitation Sciences, Iran

Abstract. [Purpose] This study compared the effectiveness of stabilization and McKenzie exercises on pain, disability, and thickness of the transverse abdominis and multifidus muscles in patients with nonspecific chronic low back pain. [Subjects] Thirty patients were randomly assigned into two groups: the McKenzie and stabilization exercise groups. [Methods] Before and after intervention, pain, disability, and thickness of the transverse abdominis and multifidus muscles were evaluated by visual analogue scale, functional rating index, and sonography, respectively. The training program was 18 scheduled sessions of individual training for both groups. [Results] After interventions, the pain score decreased in both groups. The disability score decreased only in the stabilization group. The thickness of the left multifidus was significantly increased during resting and contracting states in the stabilization group. The thickness of the right transverse abdominis during the abdominal draw-in maneuver, and thickness of the left transverse abdominis during active straight leg raising maneuver were significantly increased in the stabilization group. The intensity of pain, disability score, thickness of the right transverse abdominis during the abdominal draw-in maneuver, and thickness of the left transverse abdominis during active straight leg raising in the stabilization group were greater than those on the Mackenzie. [Conclusion] Stabilization exercises are more effective than McKenzie exercises in improving the intensity of pain and function score and in increasing the thickness of the transverse abdominis muscle.

Key words: Chronic low back pain, Stabilization exercises, Muscle thickness

INTRODUCTION

Lack of spinal core stability is supposed to be one of the important predisposing causes of recurrent low back pain (LBP). As a result, more attention has been paid to training of localized spinal stabilizer muscles in subjects with LBP. It is believed that specific stabilization exercises lead to changes in motor programming of the automatic feed-forward recruitment of deep core muscles. Therefore, stabilization exercises were suggested for chronic low back pain (CLBP) patients.

Recently, it has been reported that the use of stabilization exercises can improve the multifidus (MF) muscle size in acute LBP. However, few studies have reported the impacts of stabilization exercises on the size and function of stabilizer muscles. One study reported that the stabilization exercises led to an increase in the thickness of the stabilizer muscles. Another study showed borderline changes in contracting thickness of the TrA muscle following application of stabilization exercises. As a result, there is a lack of sufficient objective evidence about the effects of stabilization exercises on the thickness of the stabilizer muscles, especially thickness when contracted. Another approach is the McKenzie method. This approach is focused on sustained postures or repeated movements. Although McKenzie exercises could improve pain intensity in acute low back pain, subacute low back pain and CLBP, no study with regard to the effect of McKenzie exercises on the thickness of the stabilizer muscles in CLBP was found in a review of the literature.

As mentioned above, this study was carried out to determine and compare the effectiveness of stabilization and McKenzie exercises on pain, disability and TrA and MF
In this single randomized controlled trial study, the participants were selected through a simple non-probability sampling method and were randomly divided into two equal groups using sequences of random numbers. The first group (n=15) performed stabilization exercises, and the second group (n=15) performed McKenzie exercises. The examiner who assessed the outcomes was blinded to group assignment. The training program consisted of 18 sessions of supervised individual training for both groups, with the sessions performed 3 times per week for 6 weeks. Each training session lasted an hour and was performed at the Physiotherapy Clinic in the School of Rehabilitation, Tehran University of Medical Sciences, Tehran, Iran, between 2011 and 2012. Outcomes were measured in both groups before and after treatments. The study protocol was approved by the ethics committee of Tehran University of Medical Sciences. All patients provided written informed consent to participate in the study.

Thirty patients with nonspecific CLBP participated in this study on the basis of a clinical examination performed by a physician and the following inclusion criteria: age between 18–50 years, CLBP in the area between the costal margin and buttocks, with or without reference to the lower extremity (no radicular pain) that lasted more than 3 months. Patients were excluded if they had a history of recent fracture, trauma or previous surgery in the lumbar region; had spondylolysis or spondylolisthesis, spinal stenosis, neurological disorders, systemic diseases, cardiovascular diseases, diseases; were pregnant; were receiving other therapies simultaneously; had a recent fracture, trauma or previous surgery in the lumbar region; had spondylolysis or spondylolisthesis, spinal stenosis, neurological disorders, systemic diseases, cardiovascular diseases, diseases; were receiving concomitant treatment, with physical therapy modalities; or were receiving other therapies simultaneously.

After referral by a specialist, patients were reviewed based on the inclusion and exclusion criteria. Then demographic characteristics including age, sex, height, and weight were collected using a questionnaire. The pain history including the onset, location, and duration was recorded. Prior to and following the intervention, we measured pain, disability, and TrA and MF muscle thickness at rest and during contraction by visual analogue scale (VAS), Functional Rating Index (FRI) questionnaire, and ultrasound imaging, respectively.

The VAS was used for pain assessment. In this scale, pain was rated from 0 to 100 mm, in which the 0 represented no pain and 100 represented maximum pain tolerance. Subjects were asked to mark the best number indicating their pain. The data were then recorded in the questionnaire.

Disability was evaluated through the Persian version of the FRI questionnaire. The questionnaire served as a tool specifically designed for quantifying mental comprehension of function and spinal pain in the clinical conditions. The reliability and validity of the questionnaire have already been demonstrated in previous studies. The questionnaire has 10 sections, and each section was rated using the same 5-point scale. Patients scored their existing disability by choosing one of the grades (the grades ranged from 0 to 4, grade 0 meant without pain and able to complete the respective function, and grade 4 meant the maximum pain and inability to perform the functions). The overall score was calculated by the sum of the scores of all sections and was expressed by a percentage between 0 (no disability) and 100 (severe disability).

Ultrasound imaging is a reliable and reproducible method for evaluation of muscle structure, function, and activity. This method allows assessment of muscle activity by measuring changes in muscle geometry during contraction. In this study, there was high intra-tester reliability for the ultrasound measurements of the MF and TrA muscle thicknesses at rest and during contraction (ICCs= 0.87 to 0.96). To measure the thicknesses of the MF and TrA muscles, a B-mode ultrasound apparatus (MyLab 50 VXVision, ESAOTE S.p.A, Genova Italy) was used. Measurement of the thicknesses of the TrA and MF muscles was performed in a resting position and during the tasks with submaximal muscle contraction on both sides. To record the thicknesses of the TrA and MF muscles, we used an LA523 linear probe (set to 12 MHz) and a CA431 convex array probe (set to 7.5 MHz). In order to measure TrA muscle thickness, the subjects were set in crook-lying position. The ultrasound probe was placed midway between the iliac crest and costal margin, on the midaxillary line, about 10 cm off the midline of body at the level of umbilicus. TrA muscle thickness was measured in millimeters between the fascial lines, one centimeter away from the muscle junction in the direction of the thoracolumbar fascia. The two submaximal tasks were performed for the TrA muscle, the abdominal draw-in maneuver (ADIM) and active straight leg raising (ASLR). MF muscle thickness measurements were performed in the prone position with a pillow under the abdomen. The probe was placed along the spine, such that the midpoint of the probe was in line with the spinous process of the fourth lumbar vertebra. Then it was moved so that the facet joint between the fourth and fifth lumbar vertebrae was visible. This point is located directly on the MF muscle. The muscle thickness was measured from this point to the plane between the subcutaneous tissue and muscle. The submaximal task for this muscle was elevation of the contralateral arm in a prone position with a small weight (0.5 kg) on the arm, the elbow at a right angle, and the glenohumeral joint at 120 degrees of abduction.

For warming up and before performing specific exercises, participants pedaled a stationary bike for 5 minutes and then did stretching exercises for 10 minutes. Stabilization exercises were divided into 6 levels from easy to difficult. At the end of each training level, participants performed each exercise ten times for ten seconds with low intensity. During the treatment session, between 80 and 100 repetitions of the selected exercises were carried out in the McKenzie group.

The stabilization exercises were performed in 6 steps: 1) Segmental Control Exercises (SCE) with emphasis on train-
RESULTS

Demographic variables had a normal distribution. No significant difference was observed between the demographic characteristics of the two groups. The patients’ demographic characteristics are listed in Table 1. The study design and the corresponding flow diagram are shown in Fig. 1. The following data were not distributed normally after treatment: resting thickness of the left TrA, thickness of the left TrA during ADIM in the stabilization group, and resting thickness of the right TrA in the McKenzie group.

Pain decreased in both the McKenzie and stabilization groups after the intervention (p < 0.05). The disability score decreased only in the stabilization group (p < 0.05). The mean thickness of the left MF muscle when contracted, resting thickness of the left TrA muscle, thickness of the right TrA muscle during ADIM, and thickness of the left TrA during ASLR increased in the stabilization group (p < 0.05) (Table 2).

Comparison of pain, function, and thickness of the TrA and MF muscles before treatment showed no difference between two groups (p > 0.05). The changes in the pain and disability scores and right TrA muscle thickness during ADIM and the thickness of the left TrA muscle during ASLR were greater than those in the stabilization group (p < 0.05). Other variables showed no significant difference between the two groups (p > 0.05) (Table 2).

DISCUSSION

The results of this study showed that pain decreased following application of stabilization and McKenzie exercises. Disability decreased only after the application of stabilization exercises. The results indicated that the effect of stabilization exercises on pain and disability was greater than McKenzie exercises in CLBP. Also, stabilization exercises were effective in increasing the resting thickness of the left TrA muscle, the thickness of the right TrA muscle during ADIM, the thickness of the left TrA muscle during active SLR, thickness of the left MF muscle when contracted. Comparison of the effects between the two methods of exercises on muscle thickness showed that stabilization exercises were more effective than McKenzie exercises in increasing the thickness of the right TrA muscle during ADIM, and the thickness of left TrA muscle during ASLR.

Despite the borderline changes that occurred in the thickness of the TrA muscle when contracted in Vasseljen and Fladmark’s study, in the present study, the thickness of the TrA and MF muscles when contracted increased in some of the outcomes. In our study, the exercise types were different from those used in Vasseljen and Fladmark’s study. The results of this study regarding the changes in resting thickness of the TrA muscles following application of stabilization exercises were consistent with the study by Akbari et al. They showed an increase in resting thickness of the TrA and MF muscles following the application of stabilization exercises. In the present study, the resting thickness of the left TrA increased.

Table 1. Between-group baseline comparison of subjects’ characteristics

<table>
<thead>
<tr>
<th>Characteristic</th>
<th>Stabilization group</th>
<th>McKenzie group</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age (y)</td>
<td>40.1±10.8&lt;sup&gt;a&lt;/sup&gt;</td>
<td>36.6±8.2</td>
</tr>
<tr>
<td>Height (cm)</td>
<td>170.5±8.5</td>
<td>172.1±8</td>
</tr>
<tr>
<td>Weight (kg)</td>
<td>75±13</td>
<td>78.4±10.6</td>
</tr>
<tr>
<td>BMI&lt;sup&gt;b&lt;/sup&gt;</td>
<td>25.8±4.1</td>
<td>26.7±4.7</td>
</tr>
</tbody>
</table>

<sup>a</sup>BMI = body mass index, <sup>b</sup>Values are means and standard deviations
Accordingly, depending on the purpose of exercise applications, effects of exercises on the muscles can lead to hypertrophy or neuromuscular adaptation. With the emphasis placed on low-level contraction and isolation of the TrA muscles during stabilization exercises, it is expected that most of the effects of stabilization exercises are related to neuromuscular adaptation. However, muscle hypertrophy typically occurs after 8 to 12 weeks of intensive strengthening exercises. Thus, we proposed that the short duration of the present study and effects of neuromuscular adaptation led to changes in some of the outcomes.

The findings of this study are consistent with the findings of previous studies in terms of improvement in pain and function following the application of stabilization exercises. Also, stabilization exercises were found to be superior to McKenzie exercises in our study, as shown by the decreases in pain and disability, which is consistent with the results of other studies. Although stabilization exercises are the most important methods in rehabilitation of LBP disorders and in prophylaxis, the exact biological basis for the efficacy of stabilization exercises in LBP patients is not clear yet. Several mechanisms have been proposed to describe the effects of stabilization exercises on pain. These mechanisms include reduction of load and improvement in the quality of movements following improvement in co-ordination of trunk muscles. In addition, the stabilization exercises targeted the main deep muscle affected by LBP. As a result, deep muscle stabilizer muscles could influence by stabilization exercises in LBP patients. Therefore, a change in muscle thickness was only seen after stabilization exercises.

Considering the above mentioned points, pain reduction in the McKenzie group might have occurred due to other causes without changes in the thickness of abdominal and MF muscles. This approach was focused on sustained postures or repeated movements, and pain reduction might have been due to postural correction.

Therefore, both types of exercises reduced pain in patients with nonspecific CLBP. Disability was reduced only in stabilization group. Also, stabilization exercises were effective in increasing the resting thickness of the left TrA muscle, thickness of the right TrA muscle during ADIM, thickness of the left MF muscle when contracted. Stabilization exercises were more effective than McKenzie exercises in reducing pain and disability, increasing the right TrA muscle thickness during ADIM, and increasing the left TrA muscle thickness during ASLR.

**ACKNOWLEDGEMENT**

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**REFERENCES**

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**Table 2. Means and standard deviations of variables within and between group comparison**

<table>
<thead>
<tr>
<th></th>
<th>Stabilization group</th>
<th>McKenzie group</th>
</tr>
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<tbody>
<tr>
<td></td>
<td>Before</td>
<td>After</td>
</tr>
<tr>
<td>Pain (ordinal)*</td>
<td>4.33±1.58</td>
<td>1.53±1.40</td>
</tr>
<tr>
<td>Function (ordinal)*</td>
<td>39.13±15.53</td>
<td>16.66±8.59</td>
</tr>
<tr>
<td>Rt MF rest thick (mm)*</td>
<td>29.99±2.94</td>
<td>31.48±4.76</td>
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<tr>
<td>Lt MF rest thick (mm)</td>
<td>30.76±4.58</td>
<td>32.58±4.78</td>
</tr>
<tr>
<td>Rt MF cont thick (mm)</td>
<td>36.28±3.98</td>
<td>37.79±4.74</td>
</tr>
<tr>
<td>Lt MF cont thick (mm)</td>
<td>37.06±3.87</td>
<td>39.90±4.36</td>
</tr>
<tr>
<td>Rt TrA rest thick (mm)</td>
<td>3.45±0.63</td>
<td>3.85±0.75</td>
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<tr>
<td>Lt TrA rest thick (mm)</td>
<td>3.54±0.92</td>
<td>6.41±9.32</td>
</tr>
<tr>
<td>Rt TrA thick ADIM (mm)*</td>
<td>5.20±0.84</td>
<td>6.06±1.12</td>
</tr>
<tr>
<td>Lt TrA thick ADIM (mm)</td>
<td>5.65±1.00</td>
<td>11.33±20.95</td>
</tr>
<tr>
<td>Rt TrA thick ASLR (mm)</td>
<td>3.54±0.91</td>
<td>4.03±0.99</td>
</tr>
<tr>
<td>Lt TrA thick ASLR (mm)*</td>
<td>3.81±0.99</td>
<td>4.52±1.05</td>
</tr>
</tbody>
</table>

* Rt MF rest thick = right multifidus resting thickness, Lt MF rest thick = left multifidus resting thickness, Rt MF cont thick = right multifidus thickness when contracted, Lt MF cont thick = left multifidus thickness when contracted, Rt TrA rest thick = right transverse abdominis resting thickness, Lt TrA rest thick = left transverse abdominis resting thickness, Rt TrA thick ADIM = right abdominis thickness during abdominal draw-in maneuver, Lt TrA thick ADIM = left transverse abdominis thickness during abdominal draw-in maneuver, Rt TrA thick ASLR = right transverse abdominis thickness during straight leg rising, Lt TrA thick ASLR = left transverse abdominis thickness during straight rising.

b Values are means and standard deviations.

c Statistical difference at p < 0.05.

* p value for difference between groups.


