Comparison of Gait Aspects According to FES Stimulation Position Applied to Stroke Patients

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Abstract. [Purpose] This study sought to identify the gait aspects according to the FES stimulation position in stroke patients during gait training. [Subjects and Methods] To perform gait analysis, ten stroke patients were grouped based on 4 types of gait conditions: gait without FES stimulation (non-FES), gait with FES stimulation on the tibialis anterior (Ta), gait with FES stimulation on the tibialis anterior and quadriceps (TaQ), and gait with FES stimulation on the tibialis anterior and gluteus medius (TaGm). [Results] Based on repeated measures analysis of variance of measurements of gait aspects comprised of gait speed, gait cycle, and step length according to the FES stimulation position, the FES stimulation significantly affected gait aspects. [Conclusion] In conclusion, stimulating the tibialis anterior and quadriceps and stimulating the tibialis anterior and gluteus medius are much more effective than stimulating only the tibialis anterior during gait training in stroke patients using FES.

Key words: Stroke, FES, Gait

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INTRODUCTION

Gait disability among stroke patients is a very common symptom that is observed in 80% of all patients. This disability is attributed to damage due to the lesions associated with the unification function of the higher cortical and kinesthesia tract. It appears as a result of direct damage, non-activity occurring secondarily, or by non-use¹⁾. The gait aspects of stroke patients manifest with a wide variety of patterns²⁾. Generally, slow excessive force and effort are required, and coordination does not work properly. In addition, large-scale movements are noted^{1, 3)}.

Functional electrical stimulation (FES) is recently being used to establish a normal gait pattern among stroke patients. Therapeutic intervention with FES can enhance the control ability of a paretic limb within cooperative movements due to intensive enhancement of muscular strength⁴⁾. Moreover, functional electrical stimulation on a residual nerve conduction tract after damage can improve the lost exercise ability of patients⁵⁾ and can help maximize relearning of a sports activity for patients during active and repetitive movements^{6, 7)}.

In advanced research regarding gait training through FES, FES applied to a sural nerve prevents foot drop by recovering the dorsiflexion muscle at the swing phase. It is effective in increasing gait speed by decreasing the spasticity of the plantar flexion muscle⁸⁾. Lee et al.⁹⁾ stated that functional electrical stimulation on the gluteus medius contributes to a patient's daily range of motion and to independent gait by enhancing gait ability in hemiplegic stroke patients. Furthermore, Bogataj et al.¹⁰⁾ reported that treatment with electrical stimulation using a surface electrode during the acute period of stroke shows a faster effect on gait speed or coordination capability of a limb than other treatment methods. The study of Ng et al.¹¹⁾ also reported that electromechanical gait training combined with FES is more effective than general physical therapy.

Thus, changes in gait after FES application have been observed in many studies, but most studies have involved an individual muscle, and not many studies have focused on the FES stimulation position. This study aimed to examine gait aspects according to the FES stimulation position in an effort to enhance gait training in stroke patients who received FES effectively during clinical treatment.

SUBJECTS AND METHODS

Subjects

The study was conducted with 10 patients whose onset of stroke was more than 6 months previously and who had undergone hospital treatment from July 29 to August 9,

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Table 1. Effects of the FES stimulation position on gait speed, gait cycle, and step length

	Non-FES	Ta	TaQ	TaGm	Post hoc	
Gait speed (m/s)	0.47±0.13	0.53±0.15	0.61±0.16	0.59±0.16*†	a<b<c>d	
Gait cycle (cycle/s)	0.61±0.13	0.66±0.13	0.69±0.13	0.69±0.13*†	a<b<c=d	
Step length (cm)	P	42.50±8.08	45.20±8.63	50.70±6.99	48.60±6.99*†	a<b<c>d
	NP	43.00±7.87	45.60±8.51	48.80±8.61	47.60±8.24*†	a<b<c=d

Mean ± SD. Within-subjects effects: *, $p<0.05$. Between-subject effects: †, $p<0.05$. P, paretic side; NP, non-paretic side; non-FES, non-FES stimulation; Ta, FES stimulation on the tibialis anterior muscle; TaQ, FES stimulation on the tibialis anterior and quadriceps muscle; TaGm, FES stimulation on the tibialis anterior and gluteus medius muscle

2013, at D hospital located in Jeonju, Republic of Korea. The subjects could perform independent gait and had sufficient passive ranges of motion of ankle dorsiflexion that enabled the paretic ankle joint to reach either the neutral ankle angle (0°) or a minimum of 5° of plantar flexion with the knee flexed. Patients who had respiratory, cardiovascular, or orthopedic diseases were excluded from the study. All subjects understood the purpose of the study and gave written consents before participating, according to the ethical standards of the Declaration of Helsinki.

Methods

In this study, test conditions were divided into gait without FES stimulation (non-FES), gait with FES stimulation on the tibialis anterior (Ta), gait with FES stimulation on the tibialis anterior and quadriceps (TaQ), and gait with FES stimulation on the tibialis anterior and gluteus medius (TaGm) in order to evaluate gait aspects according to the FES stimulation position. Subjects slowly walked three round trips of 20 m and performed a free gait three times for a total of 20 minutes so that they could become accustomed to the changes brought about by the FES application. Gait training was not performed on the day the measurements were taken. Subjects were subjected to all 4 conditions, and gait analysis was performed for each. The order for applying the conditions was random, and a five-minute break was provided in between measurements.

In this study, a gait analysis training treadmill, Gait Trainer 2 (Biodex Medical Systems, Shirley, NY, USA, 2010), was used to examine gait speed, gait cycle, and step length, which are general components of gait. Patients were allowed to adjust the gait speed for safety and comfort considerations, and were given 3 minutes to get used to the machine. Their measurements were taken for 1 minute. Walking Man II (CyberMedic Corp., Iksan, Korea, 2010) was used for FES.

A foot switch was attached to the heel for FES so that the quadriceps and gluteus medius were stimulated when the heel come into contact with the treadmill and the tibialis anterior was stimulated when the heel lifted off the treadmill. The parameters of FES stimulation were symmetrical biphasic square waves with a pulse width of 250 μ s, while the frequency was 40 Hz. The intensity of stimulation was set just enough for the naked eye to observe contractions of the muscle.

Statistical analysis was conducted using SPSS 18.0 for

Windows. To evaluate gait aspects according to the FES stimulation position, statistical analysis with repeated measures was performed, and the LSD test was used for post hoc analysis. The significance level was set to $p<0.05$ for the statistical analysis.

RESULTS

This study was conducted with 10 subjects who were tested with FES stimulation under each of the 4 conditions identified. The general characteristics of the subjects were as follows: age, 47.80 ± 8.37 years; height, 166.00 ± 6.64 cm; weight, 65.90 ± 5.91 kg; onset, 18.90 ± 10.90 ; gender, male 7 and 3 female; diagnosis, 7 cases of hemorrhage and 3 cases of infarction; and Fugl-Meyer Assessment scale, 23.70 ± 4.42 (lower extremity motor assessment test and balance test).

In order to examine the effects of the FES stimulation position on gait components, gait speed, gait cycle, and step length among the general measurement elements were measured. Step length was measured separately on the paralyzed and non-paralyzed sides. There was a statistically significant difference in gait aspects as a result of FES stimulation depending on gait speed, gait cycle, and step length (paralyzed/non-paralyzed). The post-analysis results showed that walking with the following stimulation procedures was most effective for each element: FES stimulation on the tibialis anterior and quadriceps was most effective for gait speed, FES stimulation on the tibialis anterior and quadriceps as well as FES stimulation on the tibialis anterior and gluteus medius was most effective for gait cycle, and FES stimulation of the tibialis anterior and quadriceps on the paralyzed side and FES stimulation on the tibialis anterior and quadriceps as well as FES stimulation on the tibialis anterior and gluteus medius on the non-paralyzed side were most effective for step length (Table 1).

DISCUSSION

Among many studies aimed at improving the gait speed of stroke patients, the results of a meta-analysis of studies using FES revealed that FES is effective for enhancing gait speed¹²⁾. Based on the results of previous research, this study was conducted to examine the effect of the FES stimulation position on gait with the objective of finding the most effective stimulation position.

A study on FES stimulation and gait speed reported that functional electrical stimulation applied to the tibialis ante-

rior was effective in enhancing gait speed and cadence¹³). In a study on FES stimulation on the tibialis anterior, peroneus longus, quadriceps, and hamstring, effective movement of the knee joint of a paralyzed limb brought about by increased muscular strength and cross-sectional area of the muscle directly increased gait efficiency and gait speed¹⁴. Kim et al.¹⁵ stated that recovering the muscular strength of the hip joint abductor stabilizes the position of the hip joint, while control of the hip joint abductor is a significant element for independent gait and balance recovery; in particular, they found that the ankle dorsiflexion muscle and hip joint abductor affect gait speed¹⁶. In another study, a change in limb muscular strength reduced the dragging of the foot in the swing phase, decreasing the duration of flight of a paralyzed limb¹⁷, while gait speed increased because balance was improved due to easy movement of weight to the paralyzed side through recovery of the strength of the gluteus medius¹⁸. FES stimulation on the dorsiflexion muscle of an ankle shortens the swing phase of a paralyzed limb and increases gait speed, while FES stimulation on the quadriceps and gluteus medius leads to increased muscular strength and effective movement of joints. This in turn brings about an increased gait speed and gait cycle, which is consistent with the results of this study.

In a study on FES stimulation, balance, and confidence, Robertson et al.¹⁹ performed balance training with 15 stroke patients for 4 weeks by applying functional electrical stimulation on the dorsiflexion muscle and assessing the ABC (Activities-specific Balance Confidence Scale). The results showed that the test group that received functional electrical stimulation exhibited significant improvements. Also, Ng et al.¹¹ and Yang et al.¹⁴ reported in their studies that FES stimulation increased muscular strength and improved balance ability. Recovery of the muscular strength of the gluteus medius enhances balance as movement of weight to the paralyzed side becomes easier¹⁸, while recovery of muscular strength of the hip joint abductor acts as its stabilizer when weight is moved. This affects the recovery of dynamic balance among stroke patients²⁰. Kim et al.²¹ performed cross-sectional research on gait with FES on the gluteus medius and tibialis anterior and found that the step length of gait with FES on the gluteus medius and tibialis anterior showed a more significant increase than the step length of gait with FES on the tibialis anterior only or the step length of normal gait. The step length of gait with functional electrical stimulation on the tibialis anterior showed a more significant increase than the step length of normal gait. FES increases muscular strength and balance ability, increasing stability in the stance phase and increasing the step length of the opposite limb. This is consistent with the result of the present study, which showed that step length was increased more when the tibialis anterior was stimulated at the same time as the quadriceps or gluteus medius than when only the tibialis anterior was stimulated. In this study, the non-paralyzed side step length of gait with FES on the tibialis anterior and quadriceps showed a more significant increase than the step length of gait with FES on the tibialis anterior and gluteus medius. The increased step length of the non-paralyzed limb was associated with

an increase in gait speed. It is considered that the regulation ability of the quadriceps exerts more influence on the gait.

Thus, FES stimulation during gait training stimulates an increase in muscular strength and effective movement of joints, increasing stability in the stance phase and step length of the non-paralyzed limb. It also stimulates dorsiflexion of the ankle in the swing phase, shortening the swing phase of the affected side and increasing the gait cycle to bring about an increase in gait speed. In clinical gait training of stroke patients, stimulating the tibialis anterior along with the quadriceps and the tibialis anterior along with the gluteus medius at the same time, instead of applying FES stimulation only on the tibialis anterior, increases limb stability and would be much more effective in recovering the gait ability of patients. The only limitation of this study is that the gait analysis was conducted on a treadmill instead of a floor surface. Future research of gait on floor surface and with a larger number of subjects that also includes balance analysis is recommended.

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