Relationship between knee alignment and the electromyographic activity of quadriceps muscles in patients with knee osteoarthritis

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Abstract. [Purpose] We evaluated the relationship between knee alignment and the electromyographic (EMG) activity of the vastus medialis (VM) to the vastus lateralis (VL) muscles in patients with knee osteoarthritis (OA) in a cross-sectional study. [Subjects and Methods] Forty subjects with knee OA were assessed by anatomic radiographic knee alignment and the VM/VL ratio was calculated. Surface EMG from both the VM and VL muscles were evaluated during maximal isometric contraction at 60° knee flexion. Simultaneously, peak quadriceps torque was assessed using an isokinetic dynamometer. Subjects were categorized into low, moderate, and high varus groups according to knee malalignment. The peak quadriceps torque and VM/VL ratio across groups, and their relationships with varus malalignment were analyzed. [Results] All subjects had medial compartment OA and the VM/VL ratio of all subjects was 1.31 ± 0.28 (mean ± SD). There were no significant differences in the peak quadriceps torque or VM/VL ratios across the groups nor were there any significant relationships with varus malalignment. [Conclusion] The VM/VL ratio and peak quadriceps torque were not associated with the severity of knee varus malalignment.

Key words: Malalignment, Knee, Quadriceps

INTRODUCTION

Joint malalignment and a disproportionate axial load on the knee joint may contribute to the pathogenesis of knee osteoarthritis (OA)1), 2), although they could also be caused by the progression of OA3). An increased disproportional load on the joint in the frontal plane causes progressive cartilage loss on the medial or lateral side of the knee articular surface and bony angular deformity4). A prospective longitudinal cohort study5) demonstrated that, in primary knee OA, varus alignment increases the risk of medial OA progression (adjusted odds ratio [OR] 4.09) and valgus alignment increases the risk of lateral OA progression (adjusted OR 4.89). Additionally, varus or valgus alignment exceeding 5° at baseline was associated with greater functional deterioration over 18 months than an alignment of 5° or less.

As a biomechanical factor in the pathogenesis in knee OA, knee malalignment influences the external knee moment in the frontal plane during gait, in addition to the static load distribution across the knee joint6). Some studies have demonstrated that subjects with medial compartment knee OA walk with a greater than normal peak external knee adduction moment, and the baseline adduction moment of the knee predicted radiographic OA progression at the 6 year follow-up of patients with medial compartment knee OA7, 8). Knee alignment depends on not only bony or articular geometry, but also on the peri-articular tissues, such as joint laxity or the strength of the surrounding muscles9, 10). Although quadriceps weakness is a well-known risk factor of knee OA progression and quadriceps strengthening has been emphasized for knee OA rehabilitation, it is unclear how quadriceps strength is associated with knee malalignment. One study11) reported that the benefits of quadriceps strengthening on pain were more evident in those with more neutral alignment, while another study12) showed that greater quadriceps strength at baseline was associated with an increased likelihood of tibiofemoral OA progression in malaligned and lax knees.

This study focused on the relationship between quadriceps strength and knee alignment, and we postulated that specific strengthening of separate components of the quadriceps according to the malalignment direction would be required if the vastus medial (VM) or lateral (VL) quad-
 VM to VL activity ratio and knee alignment in subjects with knee OA. We hypothesized that the VM to VL electromyographic (EMG) activity ratio would be significantly greater in subjects with more varus malalignment than in those with a more neutral alignment.

**SUBJECTS AND METHODS**

Forty females with knee OA were recruited from the Department of Rehabilitation Medicine at Seoul St. Mary’s Hospital in South Korea. All subjects were 50 years old or over and had knee pain. They also met inclusion criterion 1) or at least two of criteria 2)–6) established by the American College of Rheumatology (ACR)14: 1) Kellgren and Lawrence (K/L) grade ≥II, 2) morning stiffness <30 min in duration, 3) crepitus on movement of the knee joint, 4) bony tenderness at the knee joint margins, 5) palpable or visible bony enlargement, and 6) no palpable warmth. Study exclusion criteria were a history of lower limb surgery or trauma, a knee injection in the preceding 2 months, a history of inflammatory arthritis, peripheral polyneuropathy, or balance or gait disturbance.

The study was approved by the Ethics Committee of the Catholic University of Korea and written consents to participation in the study was obtained from all subjects in accordance with the Declaration of Helsinki.

Radiographs were taken of a weight-bearing anteroposterior view of the most painful knee in full extension to assess joint alignment and OA severity. The subjects stood without footwear, with the tibial tubercles facing forward. Anatomic knee alignment was determined using the method of Moreland et al.15 and mechanical knee alignment was extrapolated using the regression equation of Hinman et al.16: mechanical alignment = 0.915 × (anatomic alignment) + 13.895. Anatomic alignment was measured as the angle at the intersection of the femoral and tibial anatomic axes (Fig. 1). The femoral anatomic axis was determined by drawing a line from the center of the tibial spines to a point located 10 cm proximally, midway between the medial and lateral femoral surfaces. In the same manner, the line of the tibia anatomic axis was drawn from the center of the tibial spines to a point 10 cm distally, midway between the medial and lateral tibial surfaces. In this study, the angle of knee alignment was measured as the deviation from neutral (0°) in the varus direction. OA severity was assessed using the K/L grade. All subjects were analyzed radiographically in a blinded manner by an experienced radiologist.

The peak quadriceps torque was assessed using an isokinetic dynamometer (Primus RS, BTE Technologies, Colorado) during maximal isometric contraction at 60° knee flexion. The lateral epicondyle of the femur was aligned with the axis of rotation of the dynamometer. Straps were secured firmly over the distal tibia, distal third of the thigh, and waist to limit extraneous movement. A submaximal warm-up was followed by three maximal 4-s contractions with 1-min rests between trials. The highest peak force determined by averaging the data of the three trials was multiplied by the lever length, which was then normalized by body mass (Nm/kg). The subjects were encouraged verbally, but they were blinded to the torque levels they produced.

Surface EMG recordings were performed using a Synergy EMG (Medelec, Surrey, UK) with the following equipment settings: low-frequency filter 20 Hz, high-frequency filter 1,000 Hz, and a common mode rejection ratio of over 110 dB. Before electrode placement, the skin was cleaned with alcohol to reduce signal impedance. A custom-designed disposable electrode (CareFusion, Hoechberg, Germany) was used to measure surface EMG activity. Active electrodes were placed over the motor points of the VM and VL muscles, and reference electrodes were placed over the tendons of the VM and VL, respectively. The ground electrode was positioned over the medial malleolus.

For each subject, the EMG activities were measured over the 2-s period corresponding to the time of maximum activation, during testing of peak quadriceps torque. The root mean square (RMS) value was calculated and used for the EMG amplitude17. Measurements were taken three times at 1-min intervals and the RMS average values were used in the analysis.

Statistical analyses were performed using SPSS software (ver. 11.5). First, subjects were classified into three groups based on the degree of their varus alignment: subjects with knee alignment ≤ 2 degrees varus were categorized as low varus, those with 2–4 degrees varus as moderate varus, and those ≥ 4 degrees varus were categorized as high varus18. One-way analysis of variance (ANOVA) was used to compare normally distributed variables (i.e., age, height, weight,
Table 1. Characteristics of subjects of the 3 alignment groups

<table>
<thead>
<tr>
<th></th>
<th>Entire cohort (n = 40)</th>
<th>Low varus (n = 12)</th>
<th>Moderate varus (n = 15)</th>
<th>High varus (n = 13)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age, years</td>
<td>56.7 ± 4.4</td>
<td>58.8 ± 4.6</td>
<td>56.0 ± 3.9</td>
<td>55.6 ± 4.3</td>
</tr>
<tr>
<td>Height, cm</td>
<td>154.6 ± 4.5</td>
<td>155.0 ± 5.7</td>
<td>154.9 ± 3.8</td>
<td>153.8 ± 4.3</td>
</tr>
<tr>
<td>Body weight, kg</td>
<td>57.7 ± 7.5</td>
<td>59.4 ± 7.4</td>
<td>58.8 ± 6.4</td>
<td>54.8 ± 8.4</td>
</tr>
<tr>
<td>BMI, kg/m²</td>
<td>24.1 ± 2.4</td>
<td>24.7 ± 2.0</td>
<td>24.5 ± 2.2</td>
<td>23.1 ± 2.7</td>
</tr>
<tr>
<td>Varus alignment (degrees)</td>
<td>3.2 ± 2.6</td>
<td>0.2 ± 1.3*</td>
<td>3.1 ± 0.6*</td>
<td>6.0 ± 1.9*</td>
</tr>
<tr>
<td>Pain score (NRS)</td>
<td>3.2 ± 0.7</td>
<td>3.1 ± 0.5</td>
<td>3.3 ± 0.7</td>
<td>3.1 ± 0.9</td>
</tr>
<tr>
<td>K/L grade, no.</td>
<td>I 3</td>
<td>1</td>
<td>1</td>
<td>1</td>
</tr>
<tr>
<td></td>
<td>II 23</td>
<td>7</td>
<td>9</td>
<td>7</td>
</tr>
<tr>
<td></td>
<td>III 11</td>
<td>4</td>
<td>3</td>
<td>4</td>
</tr>
<tr>
<td></td>
<td>IV 3</td>
<td>0</td>
<td>2</td>
<td>1</td>
</tr>
<tr>
<td>Quadriceps torque, Nm/kg</td>
<td>1.10 ± 0.33</td>
<td>1.14 ± 0.37</td>
<td>0.99 ± 0.31</td>
<td>1.17 ± 0.32</td>
</tr>
<tr>
<td>VM/VL ratio</td>
<td>1.31 ± 0.28</td>
<td>1.31 ± 0.27</td>
<td>1.31 ± 0.31</td>
<td>1.30 ± 0.28</td>
</tr>
</tbody>
</table>

Values are the mean ± SD unless otherwise indicated.
BMI: body mass index; NRS: numeric rating scale; K/L: Kellgren/Lawrence; no: number; VM: vastus medialis; VL: vastus lateralis.
* Significant difference, p < 0.05.

Table 2. Quadriceps measurements of the 3 alignment groups adjusted for age and disease severity

<table>
<thead>
<tr>
<th></th>
<th>Least varus (n = 12)</th>
<th>Moderate varus (n = 15)</th>
<th>Most varus (n = 13)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Quadriceps torque, Nm/kg</td>
<td>1.10 ± 0.10</td>
<td>1.01 ± 0.09</td>
<td>1.19 ± 0.09</td>
</tr>
<tr>
<td>VM/VL ratio</td>
<td>1.21 ± 0.08</td>
<td>1.36 ± 0.06</td>
<td>1.35 ± 0.07</td>
</tr>
</tbody>
</table>

Values are expressed as adjusted mean ± SE unless otherwise indicated.
VM: vastus medialis; VL: vastus lateralis. *Significant difference, p < 0.05.

Table 3. Association between quadriceps measurements and knee alignment as determined by regression analyses adjusted for age and disease severity

<table>
<thead>
<tr>
<th></th>
<th>B</th>
<th>R²</th>
</tr>
</thead>
<tbody>
<tr>
<td>Quadriceps torque, Nm/kg</td>
<td>−0.001</td>
<td>0.066</td>
</tr>
<tr>
<td>VM/VL ratio</td>
<td>3.224</td>
<td>0.141</td>
</tr>
</tbody>
</table>

B: unstandardized regression coefficient.
VM: vastus medialis; VL: vastus lateralis. *Significant difference, p < 0.05.

RESULTS

The characteristics of the 40 subjects are summarized in Table 1. There were no significant differences in age, height, body weight, body mass index, NRS, or K/L grade among the groups (p > 0.05). All subjects had medial joint space narrowing greater than lateral joint space narrowing on visual inspection. The VM/VL ratio of all subjects averaged 1.31 ± 0.28 (mean ± SD). There were no significant differences in the peak quadriceps torque or VM/VL ratio among the groups after adjusting for age and disease severity (Table 2). There was no significant relationship between the peak quadriceps torque or VM/VL ratio and varus malalignment after adjusting for age and disease severity (Table 3).

DISCUSSION

Although we hypothesized that the VM/VL ratio would be significantly greater in subjects with greater varus malalignment than in those with a more neutral alignment, there
were no significant associations between the VM/VL ratio and the knee varus alignment categories. However, the EMG activity of the VM was greater than that of the VL, with the mean VM/VL ratio being approximately 1.3. This is consistent with the results of a recent study\textsuperscript{12}, in which the VM/VL ratio of the cross-sectional area obtained by MRI was higher in a genu varum group than in a neutral or genu valgum group. A previous study showed that the ratio of VM oblique to VL EMG activity during knee flexion-extension movement in subjects with no knee pain was almost 1.1\textsuperscript{19}. However, we cannot directly compare our results with these results because we evaluated the VM/VL ratio of knee OA patients during maximal isometric contraction, and most of them had varus alignment. Thus, further study including OA patients with valgus alignment is needed.

There were no significant differences in the peak quadriceps torque and pain score (VAS) among the groups, which is a finding similar to that reported in a recent study\textsuperscript{18}. The mean isometric strength at 60° knee flexion of our subjects was 1.1 Nm/kg, which was similar to that reported by Lim et al.\textsuperscript{18}, considering that our study included only female patients. However, there was no significant correlation between the peak quadriceps torque and varus malalignment, in contrast to a previous study\textsuperscript{18} which reported that knee alignment accounted for a small, but significant proportion of the variance in quadriceps strength. It is unclear why our findings differed from this result. There are several possible reasons. First, the number of subjects was small, and it may have been insufficient to show a correlation between the peak quadriceps torque and varus malalignment. Second, the distribution of alignment was somewhat narrow, most of the subjects had moderate varus malalignment, of 2–5 degrees, and only five patients had mild valgus alignment. Third, a potential health-based selection bias could exist, because volunteers with knee OA were recruited for our study and they had active life styles, which might have lessened the differences in quadriceps activities across the groups.

The roles of joint malalignment have not been clearly determined for knee OA progression. Knee malalignment might cause progressive cartilage loss, further progression of unilateral compartment OA, and a decline in physical function after as little as 18 months of observation\textsuperscript{4, 5}. Malalignment might disturb the normal transmission of force across the knee by shifting the load-bearing axis, the line drawn from the middle of the femoral head to the middle of the ankle. This line passes medial or lateral to the knee in varus or valgus malalignment, respectively\textsuperscript{20}. Disproportionate loading of the knee joint during static postures can be increased by dynamic activities, such as gait. Osteoarthritic changes in the knee joint commonly involve the medial compartment, so varus malalignment is more common than valgus malalignment, as seen in our study. As noted above, varus malalignment may further increase the medial load during gait\textsuperscript{21} with increased adduction moment, contributing to the progression of medial compartment knee OA\textsuperscript{4-6}.

Mechanical stress generated from geometric alignment induces specific muscle loading, which may elicit hypertrophy of that muscle. In our study, the VM activity was greater than the VL activity in all but two subjects. An exploration of whether the VM/VL ratio is associated with varus or valgus alignment is important for knee OA rehabilitation. Quadriceps strengthening has long been emphasized for knee OA rehabilitation. However, there is some evidence that generic quadriceps strengthening is not always helpful for knee OA, especially in patients with knee malalignment. Sharma et al.\textsuperscript{12} revealed that greater absolute quadriceps strength in people with malaligned knees may have deleterious consequences in terms of primary knee OA progression. With malalignment, the muscle force is not generated on the joint structures evenly and the extensor muscles might function less efficiently than with a normally aligned knee\textsuperscript{22}. Thus, specific muscle training rather than a generic strengthening program is required for knee OA rehabilitation.

If a relationship exists between knee alignment and the VM/VL ratio, it would provide evidence in support of the development of specific strengthening programs tailored to knee alignment. Although we found no correlation between knee alignment and the VM/VL ratio, the VM/VL ratio was high in the subjects who had varus alignment. To our knowledge, this is the first study to examine the relationship between the VM/VL ratio and knee alignment.

Our study had several limitations. First, we did not obtain full-limb radiographs to determine mechanical alignment. Although the tibia or femur anatomic axis can be mistaken with a bow curvature, a good to excellent correlation between the anatomic and mechanical axes (r = 0.65–0.88) has been reported\textsuperscript{16, 23}. Thus, it seems unlikely that our results would change with use of the mechanical axis. Second, our study had a cross-sectional design, so a cause-and-effect relationship could not be inferred from our present results. Third, as mentioned above, the number of subjects in our study was small and the distribution of alignment was narrow.

Future studies should evaluate more subjects, including patients with valgus alignment. More dynamic analyses are needed to confirm the relationship between the VM/VL ratio and knee alignments during walking or jogging, and the effects of separate quadriceps muscle strengthening on malalignment should also be evaluated.

In conclusion, neither the VM/VL ratio nor the peak quadriceps torque were not associated with the severity of knee varus malalignment.

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**REFERENCES**


