Original Article

Comparative assessment of knee extensor and flexor muscle strength measured using a hand-held vs. isokinetic dynamometer

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Abstract. [Purpose] To compare measurements of knee extensor and flexor muscle strength performed using a hand-held dynamometer and an isokinetic dynamometer in apparently healthy subjects. [Subjects and Methods] Thirty adult volunteers underwent knee muscle strength evaluation using an isokinetic or a hand-held dynamometer. [Results] Strong positive correlations were found between the 2 methods, with correlation coefficients r ranging from 0.72 (95% confidence interval [CI], 0.48–0.86) to 0.87 (95% CI, 0.75–0.94), depending on the muscle group and the isokinetic evaluation mode. The reproducibility of the hand-held dynamometer findings was good, judged by a coefficient of variation of 3.2–4.2%. However, the correlation between the 2 methods for the assessment of flexor/extensor ratios ranged from -0.04 to 0.46 . [Conclusion] Knee extensor and flexor muscle strength recorded with a hand-held dynamometer is reproducible and significantly correlated with the isokinetic values, indicating that this method may in some cases be a useful replacement for isokinetic strength measurement. However, for strength ratio assessment, and when judged against the isokinetic standard, a hand-held dynamometer is not a valid option.

Key words: Muscle, Strength, Dynamometer

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INTRODUCTION

Numerous pathological conditions can lead to alterations in muscle performance and locomotor ability^{1–7)}. The strength of the knee extensor and flexor muscles has been extensively studied and is a relevant clinical indicator of health status and functional capacity in coronary artery disease⁸⁾, neuromuscular diseases⁹⁾, the elderly¹⁰⁾, renal disease¹¹⁾, and fibromyalgia¹²⁾. In sports medicine, knee extensor and flexor muscle strength is often monitored with the aim of preventing or treating orthopedic as well as muscular injuries^{13–19)}. Therefore, practitioners need to have reliable tools for easy and reproducible assessment of muscle strength. The isokinetic concept of exercise²⁰⁾ is currently considered the best method for the assessment of knee extensor and flexor strength because of its well-established validity and reproducibility^{21–25)}. However, the acquisition and maintenance costs, the time required to perform an isokinetic assessment, as well as the absence of portability of isokinetic dynamometers can limit their use. Conversely, hand-held dynamometers (HHD) are characterized by specific features such as low cost, portable design, and rapid data acquisition. These systems are increasingly used, both in the clinic

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and in research. An HHD provides reliable and reproducible results when used for the evaluation of muscle groups that produce little or moderate amounts of force. However, the results obtained for strong muscles, such as the knee extensors, are less convincing^{26–28}). A systematic review comparing muscle strength assessment by HHD and isokinetic testing²⁹) showed a positive correlation between these methods. However, the heterogeneity of the protocols and devices evaluated made the interpretation of the results difficult. Therefore, the aim of this study was to: 1) assess the validity of HHD vs. isokinetic dynamometry in the evaluation of knee extensor and flexor muscle strength, 2) establish the reproducibility of HHD measurements of knee extensor and flexor muscle strength, and 3) compare the flexor/extensor ratios obtained with the 2 methods.

SUBJECTS AND METHODS

The study was carried out at the Muscle Evaluation Unit at the Clemenceau Rehabilitation University Institute (Strasbourg, France) and involved 30 healthy volunteers (Table 1).

Subjects were recruited by means of advertisement in the university network from January 2015 to November 2015. Inclusion criteria were as follows: age older than 18 years, and without cardiovascular disorders, osteoarticular diseases of the knees, or previous knee osteoligamentous or thigh muscle injuries.

The study protocol was approved by the local ethics committee. All participants were fully informed about the risks and procedures associated with the experiment and provided written informed consent to participate in the study. The trial registration number on ClinicalTrials.gov is ID: NCT02566122.

Each participant completed a 10-min warm-up on a cycle ergometer (power: 1 W/kg body weight; pedaling rate: 70–80 rpm). The testing method sequence (HHD vs. isokinetic testing) was established according to a randomization table prepared by the Biostatistics Department of the Strasbourg University Hospitals using R software version 3.2.2 (R Core Team (2015). R Foundation for Statistical Computing, Vienna, Austria. URL <https://www.R-project.org/>). The randomization of the subjects was generated by a draw using a Bernoulli distribution with a parameter of 0.5 to maintain a mean balance in the test order. The randomization was simple, without any blocking variable. A recovery period of 20 min was implemented between testing methods. For both methods, muscle strength was first measured in the dominant leg, and after a 10-min rest, in the non-dominant leg. To avoid inter-examiner variations, all measurements were carried out by a single investigator, specialized in Physical Medicine and Rehabilitation (male, 31 years old, 180 cm, and 90 kg).

The strength of the extensor and flexor muscles of both knees was assessed using an isokinetic dynamometer (Con-Trex MJ; CMV AG, Dübendorf, Switzerland). Each participant was positioned on an adjustable chair with the back set at 90° of posterior inclination. The sitting position was set according to the manufacturer's recommendations. The knee range of motion was set at 90° (from 100° to 10° of flexion; 0° corresponding to the complete extension of the knee) after having aligned the leg segment to anatomical zero. Finally, a measurement of gravity for the leg segment to be tested was carried out over the entire range of motion. The protocol of isokinetic evaluation included 6 series of contractions on the dominant and non-dominant sides including concentric, isometric, and eccentric evaluations of the knee extensor and flexor muscles (Table 2). A recovery period of 60 s was observed between each maximal series. Before each maximal series, participants carried out a «trial» submaximal series to become familiar with the contraction mode and the angular speed. Participants did not have any visual feedback of their performance. Before the test, participants received standardized oral information on the experimental procedure and were verbally encouraged in a standardized manner by the operator during the test. Following 10 min of rest after the evaluation of the dominant leg, muscle testing was performed in exactly the same way for the non-dominant side.

The strength of the extensor and flexor muscles of both knees was assessed with hand-held dynamometry (MicroFET2®, Hogan Health Industries, Inc., UT, USA). This dynamometer is a portable digital instrument than can be held in the palm of the hand giving muscle strength measurements in kilogram-force (kgf). As with manual muscle testing, this dynamometer is placed between the leg segment to be evaluated and the examiner's hand. Participants were asked to sit with their legs dangling over the end of a standard, adjustable examination table, with hips and knees flexed to 90°, in order to have a distance of 1–2 cm between the popliteal fossae and the table end. The height of the examination table was adjusted to have a distance of about 10 cm between the participant's feet and the floor. Participants had to hold the side-edges of the table with their hands and carry out a maximal isometric voluntary contraction for 5 s. The examiner positioned a knee on the floor, with the arm fully extended in front of the lower limb to be tested. To evaluate the knee extensor muscles, the dynamometer was placed on the anterior part of the lower leg, above the talotibial joint line (Fig. 1.A). The examiner placed one of his feet against the wall to better resist muscle contraction. To evaluate the knee flexor muscles, the dynamometer was placed on the posterior part of the leg, 1–2 cm above the lateral malleolus (Fig. 1.B). In both cases, the examiner produced a resistance force in the horizontal direction to counter the force developed by the participant and maintain an isometric contraction of the knee extensor and flexor muscles. The evaluation started with the extensor muscles of the dominant leg, followed by the flexors of the dominant side. After a recovery period of 10 min, the knee extensor and flexor muscles of the non-dominant leg were assessed using the same experimental design. For each muscle group, participants carried out 3 isometric maximal voluntary contractions of 5 s. A 60-s recovery period was observed between each muscle contraction. The position of the leg to be tested was verified initially with the help of a standard goniometer. Before the evaluation, participants received standardized oral information on the test procedure and were encouraged orally during the test.

For each isokinetic series, the measurement criterion was the peak torque (PT) obtained during each series, expressed in

Table 1. Characteristics of the population (n=30)

	Mean $\pm$ SD	Range
Age (years)	32.8 $\pm$ 11.5	20–59
Height (cm)	176.9 $\pm$ 10.3	160–197
Weight (kg)	74.5 $\pm$ 15.8	52–109
Gender	Males (n=20)	Females (n=10)
Laterality	Right (n=27)	Left (n=3)
Test sequence	ISO then HHD (n=16)	HHD then ISO (n=14)

ISO: isokinetic dynamometer; HHD: hand-held dynamometer

Fig. 1. Position of an individual subject for the evaluation of knee-extensor (panel A) and Knee-flexor (panel B) muscles using the hand-held dynamometer**Table 2.** Protocol for muscle strength measurement with the isokinetic dynamometer

Series	Speed	Muscles	Mode	Repetitions	ROM/position
Warm-up	180°/sec	Ext/Flex	Concentric	10	90°
Warm-up	120°/sec	Ext/Flex	Concentric	10	90°
Series 1	60°/sec	Ext/Flex	Concentric	3	90°
Series 2	180°/sec	Ext/Flex	Concentric	6	90°
Series 3	0°/sec	Ext	Isometric	1	90° of flexion
Series 4	0°/sec	Flex	Isometric	1	90° of flexion
Series 5	60°/sec	Ext	Eccentric	3	90°
Series 6	60°/sec	Flex	Eccentric	3	90°

Ext: knee extensors; Flex: knee flexors; ROM: range of motion

Newton-meters (Nm).

The maximal force developed during each contraction, expressed in kilogram-force (kgf), was recorded. For each muscle group, the maximal force was averaged over the 3 isometric contractions and used as the measurement criterion.

Thus, the 2 obtained variables were the peak torque (Nm) and the maximal force (kgf).

By assuming a correlation of 0.6 between the 2 measurements and a total magnitude of the confidence interval of 0.45 around the estimate, a sample size of 28 subjects was needed. The reproducibility of the HHD measurement was established using the coefficient of variation over 3 consecutive measures. According to Stokes, reproducibility was considered acceptable when the coefficient of variation was 15% or below³⁰. The statistical analysis was performed independently by the Biostatistics Department of the Strasbourg University Hospitals. All analyses were carried out using R version 3.2.2, with all the required packages, in the most updated version available at the time of the data analysis. The Gaussian character of the variables was assessed with the Shapiro-Wilk test. When 2 variables followed a normal distribution, the Pearson correlation coefficient was used; if not, the Spearman correlation coefficient was employed. Concerning the correlations, the «test sequence» and the «laterality» effects were evaluated by ensuring that the confidence intervals (CI) at 95% for each variable were overlapping in the 2 modalities. Values are presented as mean $\pm$ SD unless otherwise indicated.

RESULTS

No «test sequence» or «laterality» effect was found. The results obtained with the 2 evaluation modes on the whole population are summarized in Table 3. The strengths measured for the knee extensor muscles were greater than the corresponding values for the knee flexor muscles, whatever the mode and velocity of the muscle actions ($p < 0.05$).

The knee flexor/extensor strength ratios did not change according to the evaluation mode, with no difference between the dominant and non-dominant sides (Table 4).

The knee extensor muscle strength was significantly greater than for the knee flexor muscles, both on the dominant and non-dominant side ($p < 0.05$). There was no difference between the dominant and non-dominant side in a given muscle group (Table 3). The ratios of knee flexor/extensor muscle strength were similar in dominant and non-dominant sides and were not significantly different compared to isokinetic ratios (Table 4).

The coefficient of variation of the 3 isometric muscle strength measurements using the microFET 2 HHD ranged from

Table 3. Results of the muscle strength measurements

	Mean $\pm$ SD Ecart-type	Range	Median
Isokinetic (Nm)			
Concentric 60°/sec			
EXT D	179.1 $\pm$ 52.2*\$\$	100.3–275.8	180.7
EXT ND	165.4 $\pm$ 52.0*	90.5–260.3	155.3
FLEX D	91.9 $\pm$ 28.5\$	51.1–164.7	93.8
FLEX ND	85.1 $\pm$ 25.5	51.0–143.8	78.1
Concentric 180°/sec			
EXT D	132.3 $\pm$ 39.4*\$	75.4–207.8	136.8
EXT ND	130.4 $\pm$ 39.6*	71.5–204.2	134.1
FLEX D	72.2 $\pm$ 22.9\$	32.1–115.3	72.8
FLEX ND	71.8 $\pm$ 24.1\$	32.0–141.6	69.2
Isometric 0°/sec			
EXT D	177.2 $\pm$ 57.3*	89.5–291.8	181.2
EXT ND	167.4 $\pm$ 56.6*	88.0–281.0	162.2
FLEX D	84.0 $\pm$ 25.2	48.0–153.7	84.7
FLEX ND	79.3 $\pm$ 25.9	45.0–144.2	73.1
Eccentric 60°/sec			
EXT D	201.9 $\pm$ 61.9*	110.9–357.5	191.5
EXT ND	195.5 $\pm$ 69.8*	111.8–357.0	169.9
FLEX D	123.1 $\pm$ 44.1	69.5–252.3	111.6
FLEX ND	116.7 $\pm$ 36.8	65.9–210.3	103.8
HHD (kgf)			
EXT D	52.9 $\pm$ 16.7*	22.7–87.4	57.6
EXT ND	51.1 $\pm$ 17.2*	22.2–84.3	51.8
FLEX D	26.7 $\pm$ 6.0	17.4–40.9	27.2
FLEX ND	26.9 $\pm$ 5.3	18.2–38.9	27.1

EXT: knee extensors; FLEX: knee flexors; D: dominant side; ND: non-dominant side; SD: standard deviation. * $p < 0.05$ in EXT vs. FLEX in similar conditions. \$ $p < 0.05$ vs. Eccentric 60°/s in similar muscles. # $p < 0.05$ Concentric 60°/s vs. concentric 180°/s in similar muscles

Table 4. Flexor/Extensor ratios in isokinetic and hand-held dynamometry

	Dominant Side	Non dominant Side
Concentric 60°/sec	52 $\pm$ 7.0%	53 $\pm$ 9.7%
Concentric 180°/sec	55 $\pm$ 7.0%	55 $\pm$ 8.4%
Isometric 0°/sec	49 $\pm$ 8.7%	49 $\pm$ 11.0%
Eccentric 60°/sec	61 $\pm$ 8.1%	61 $\pm$ 10.9%
HHD	53 $\pm$ 12.9%	57 $\pm$ 14.6%

Data are means $\pm$ SD. HHD: hand-held dynamometer

3.2 to 4.2% according to the muscle group evaluated. Mean difference (absolute and relative values) as well as limits of agreement were similar between muscle groups (Table 5).

The correlation coefficient between the isokinetic and HHD muscle strength values ranged from $r = 0.87$ (0.75–0.94) to $r = 0.72$ (0.48–0.86) ($p < 0.01$), indicating that the correlation between testing methods was generally good (Table 6).

The flexor/extensor ratios were significantly correlated between the HHD and isokinetic dynamometer in concentric 180°/sec and isometric 0°/sec modes on the dominant and non-dominant sides ($p < 0.05$). The flexor/extensor ratio measured in concentric 60°/sec mode was correlated to the HHD only for the non-dominant side. No correlation was observed for the flexor/extensor ratios between HHD and isokinetic eccentric –60°/sec mode (Table 7).

DISCUSSION

The results of the present study show: 1) good reproducibility of the HHD for knee extensor/flexor muscle strength assessment, 2) clinically acceptable agreement between the values obtained with the HHD versus the isokinetic dynamometer, and 3) the need for caution when interpreting the flexor/extensor ratios using HHD compared to isokinetic dynamometry.

The muscle strength values using isokinetic dynamometry recorded in this study are in good agreement with those found in the literature³¹⁾, particularly in the study by Maffiuleti et al. in 2007²³⁾. For a similar population of healthy individuals (age: 30 $\pm$ 5 vs. 33 $\pm$ 11 years old; height: 175 $\pm$ 8 vs. 177 $\pm$ 10 cm; weight: 70 $\pm$ 13 vs. 74 $\pm$ 16 kg), the strength measurements using the Con-Trex isokinetic module were very close, with a peak torque for the knee extensors on the dominant side of 178 $\pm$ 46 vs. 179 $\pm$ 52 Nm (concentric at 60°/s); 132 $\pm$ 38 vs. 132 $\pm$ 39 Nm (concentric 180°/s), and 202 $\pm$ 68 vs. 202 $\pm$ 62 Nm (eccentric 60°/s) when compared with our values.

Table 5. Reproducibility of muscle strength evaluation with microFET 2 hand-held dynamometer

	Coefficient of variation	Mean Difference		Limits of agreement	
	(%)	(kgf)	(%)	(kgf)	(%)
Dominant Knee Extensors	3.2	0.1 ± 3.7	0.1 ± 7.0	-7.3–7.6	-13.8–14.0
Non-dominant Knee Extensors	3.3	0.0 ± 3.7	0.4 ± 7.4	-7.5–7.5	-15.1–14.4
Dominant Knee Flexors	4.2	0.4 ± 2.5	1.4 ± 8.9	-4.6–5.4	-16.4–19.2
Non-dominant Knee Flexors	3.7	0.3 ± 2.1	0.9 ± 7.7	-3.9–4.6	-14.4–16.3

Table 6. Correlation coefficients and 95% confidence intervals for knee muscle strength assessments obtained by hand-held (HHD) and isokinetic dynamometers (Con-Trex)

	Con-Trex			
	Eccentric	Isometric	Concentric	Concentric
	60°/sec	0°/sec	60°/sec	180°/sec
HHD				
Extensors D	r=0.87 (0.75–0.94)	r=0.85 (0.70–0.92)	r=0.87 (0.73–0.93)	r=0.85 (0.71–0.93)
Extensors ND	r=0.84* (0.69–0.92)	r=0.87 (0.74–0.94)	r=0.86 (0.72–0.93)	r=0.87 (0.74–0.94)
Flexors D	r=0.80* (0.62–0.90)	r=0.75 (0.53–0.87)	r=0.81 (0.63–0.91)	r=0.85 (0.70–0.93)
Flexors ND	r=0.75* (0.53–0.87)	r=0.72* (0.48–0.86)	r=0.83* (0.67–0.92)	r=0.82 (0.66–0.91)

*Spearman correlation coefficient; D: dominant side; ND: non-dominant side. All coefficients of correlation are significant ($p < 0.01$).

Table 7. Coefficients of correlation for knee flexor/extensor muscle strength ratios obtained with hand-held or isokinetic dynamometry

	Dominant	Non dominant
Concentric 60°/sec	0.23	0.46 *
Concentric 180°/sec	0.39 *	0.45 *
Isometric 0°/sec	0.37 *	0.46 *
Eccentric 60°/sec	-0.04	0.13

* $p < 0.05$

Similarly, the muscle strength values recorded with the HHD are in agreement, albeit with greater absolute data, with literature data^{32, 33}) and with the recent study by Douma et al., who established reference values for knee extensor and flexor muscle strength in the active Dutch population by using the MicroFet 2 HHD³⁴). The magnitude of difference between our values and previously published data using HHD is likely related to the characteristics of the participants, who were younger and fitter in our study compared to previous studies.

Greater limits of agreement were previously observed for reproducibility of muscle strength using HHD in strong muscle groups (i.e., knee extensors) compared to weaker muscle groups (i.e., knee or elbow flexors)³⁴). Consequently, HHD was not considered as suitable methodology for muscle strength assessment in knee extensors³⁵). Conversely, our results are at odds with this view as we report that the reproducibility of muscle strength assessment is not altered by the level of muscle strength developed by the subjects. Indeed, the variation coefficients were lower for the 3 measures of knee extensors compared to knee flexors, despite higher levels of absolute strength in the former. Similarly, we did not observe greater limits of agreement (LOA) in the knee extensors compared to the knee flexors. Of note, absolute values of LOA in the present study are somewhat lower than those previously published³⁴). We suggest that if HHD devices are manipulated by experienced operators, HHD can be used for the evaluation of muscle strength, even in strong muscles such as the knee extensors. It should also be kept in mind that the strength of the operator might be key in stabilizing the HHD device during the measurement procedure, and therefore the operator's own strength is likely to be of great importance for the accuracy of the measurements³⁶).

When compared with previous results reporting the coefficient of variation (CV) of isokinetic measurements using a ConTrex device (1.9–3.4% for knee extensors and 2.7–3.6% for knee flexors), the CVs reported in the present study are very similar for HHD (3.2–3.3% for knee extensors and 3.7–4.2% for knee flexors). This result suggests that the reproducibility of the strength measurements using HHD is in close agreement with that observed with isokinetic testing²³).

In a previous literature review comparing HHD with isokinetic dynamometry, Stark et al. showed that correlation coefficients ranged between 0.43 and 0.99 for the knee extensor and flexor muscles²⁹). However, the heterogeneity of the protocols as well as the different models of dynamometers make the results difficult to interpret. The present study is the first to analyze the correlation between these specific dynamometers (ConTrex isokinetic vs MicroFet 2), and we report a good correlations between the 2 methods ($r=0.72-0.87$). Of note, the present data were gathered using a simple protocol, easily reproducible without any additional equipment, in order to be established in routine clinical practice and to take the greatest advantage of the practical aspects of HHD.

When looking at subjects engaged in regular sports practice, only one study previously explored the correlation between HHD and isokinetic measurements³⁷). The study reported lower correlation coefficients ($r=0.334 \pm 0.11-0.617 \pm 0.7$) compared to our results, but it should be emphasized that the number of subjects, the type of dynamometers, and the protocol employed were different.

Lastly, the present study is also the first to provide a correlation analysis between HHD and isokinetic testing for the evaluation of knee flexor/extensor muscle ratios, an index used routinely in the field of sports medicine. Our results show correlation coefficients ranging from 0.37 to 0.46 (all $p<0.05$). Although statistically significant, these results indicate a moderate level of correlation between the 2 methodologies, and even no correlation at all when comparing flexor/extensor ratios obtained using HHD with that from isokinetic testing in eccentric mode. Therefore, flexor/extensor muscle strength ratios measured using HHD should be interpreted with caution until further investigation is performed in this area.

A limitation of our study is the fact that our population consisted of healthy, relatively young volunteers without osteo-articular or neuromuscular pathologies. Deones et al. compared muscle strength measurements by using hand-held and isokinetic dynamometers in a population of individuals with various unilateral orthopedic pathologies of the knee⁵). They found a significant correlation between both methods (r ranging from 0.57 to 0.80). However, the evaluation by HHD did not highlight a statistically significant difference between sides, whereas the isokinetic evaluation found a force deficit on the injured side. The pain that the patient may experience during the evaluation could be a confusing factor and must be taken into account when interpreting the strength results in the presence of pathologies. Another limit of this work is that HHD and isokinetic devices do not provide strength assessment with similar units of measurement. This makes direct comparison of absolute strength values difficult and limits the present comparison to correlation analysis. To obtain strength values expressed in the same units between the 2 devices (Newtons or kgf) would have required an evaluation of the lever arm, which is likely to have introduced more variability in the data.

Each evaluation method has its specific advantages and limitations. For a practitioner looking for rapid and regular muscle strength testing, the HHD allows rapid and easy acquisition of objective strength measurements. Knee extensor and flexor muscle strength recorded with an HHD is reproducible and significantly correlated with the isokinetic values, indicating that this method may in some cases be a useful replacement for isokinetic strength measurement, even for the assessment of strong muscles. However, for strength ratio assessment, and when judged against the isokinetic standard, HHD is not a valid option.

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